# ORIGINAL RESEARCH

# Albumin exfoliated titanium disulfide nanosheet: a multifunctional nanoplatform for synergistic photothermal/radiation colon cancer therapy

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Purpose: TiS<sub>2</sub>-HSA-FA, a nanoagent based on titanium disulfide (TiS<sub>2</sub>), human serum albumin (HSA), and folic acid (FA), was synthesized for potential use in synergistic photothermal/radiation therapy for colon cancer.

Methods: TiS<sub>2</sub> nanosheets were synthesized through a HSA-assisted exfoliation method and then modified with PEGylated FA. The morphology, size, zeta potential, stability, cellular uptake, cytotoxicity, biodistribution, and in vitro and in vivo biocompatibility of the nanoparticles as well as their suitability for synergistic photothermal/radiation colon cancer therapy were investigated.

**Results:** The as-synthesized TiS<sub>2</sub>-HSA-FA nanoparticles showed excellent physiological stability, as well as high absorption values in the near-infrared (NIR) and X-ray regions, giving them superb activity as a photothermal and radiation sensitizer. In vitro and in vivo experiments indicated that TiS2-HSA-FA showed high tumor targeting selectivity, blood circulation time, biocompatibility, and suitability for synergistic tumor photothermal radiotherapy.

Conclusion: A multifunctional nanoplatform based on TiS2 was developed and found to be potentially suitable for synergistic photothermal/radiation therapy for colon cancer.

Keywords: titanium disulfide, tumor target, photothermal therapy, radiotherapy, synergistic colon cancer therapy

# Introduction

Although anti-tumor therapeutics have greatly improved in recent decades, malignant tumors are still a major threat to human beings' health worldwide.<sup>1,2</sup> One of the most commonly used treatment strategies is radiotherapy (RT), in which tumors are exposed to ionizing radiation such as X-rays in an attempt to produce necrosis of tumor tissue through DNA damage and generation of reactive oxygen species.<sup>3-5</sup> However, in practice, RT has several drawbacks. One is that it can harm normal tissue and thereby induce acute side effects such as nausea and vomiting, hair loss, etc.<sup>6,7</sup> Another is that considerable dose must be used to ensure that all tumor cells are killed, and yet X-ray irradiation has no tumor specificity. This necessitates excessively large radiation doses, inevitably causing injury to healthy tissues. To overcome these drawbacks, a series of radio-sensitizers such as the two-dimensional (2D) lavered transition metal dichalcogenides (TMDs) (MoS<sub>2</sub>, WS<sub>2</sub>, MoSe<sub>2</sub>, and ReS<sub>2</sub>) and other inorganic materials have been prepared.<sup>8-13</sup> Most TMDs were reported to contain high-Z elements that can act as radio-sensitizers to promote the cancer RT

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effect by absorbing X-rays and concentrating the radiation dose within tumors.<sup>14–16</sup> For example, Shen and co-authors have prepared uniform ultrathin rhenium disulfide nanosheets for photothermal RT.<sup>16</sup> However, the hypoxic environment inside tumors is still considered a major challenge for successful use of radio-sensitizers in RT.<sup>17,18</sup>

Photothermal therapy (PTT) has attracted substantial interest of late, as an alternative tumor treatment strategy.<sup>19,20</sup> It is minimally invasive, and its high specificity means minimal side effects in normal tissues. PTT relies on photothermal agents to convert absorbed light energy into heat to kill tumor cells.<sup>21-23</sup> Recently, various nanomaterials such as organic small molecules,<sup>24,25</sup> TMDs-based nanocomposites,<sup>19,26</sup> protein-based nanoparticles,<sup>27,28</sup> etc. have been developed as PTT nanoagents.<sup>29-31</sup> Among these, TMD-based nanoagents have demonstrated great potential for PTT because of their strong absorbance in the near IR (NIR) region and their large specific surface area which facilitates their functional modification. In addition, under NIR laser irradiation, TMD-based nanoagents can increase intratumor blood circulation, thereby facilitating oxygen availability inside the tumor, which could facilitate the RT effect.<sup>16,32,33</sup> It is, therefore, thought that some type of TMD nanomaterial could be found which could act as an "all in one" nanoagent, perfectly combining RT and PTT for optimal therapeutic effect.

In this work, we prepared a new multifunctional nanoagent for combined PTT and RT, using tumor-targeted molecule FA and PEG modification of albumin exfoliated TiS2 nanosheets (TiS<sub>2</sub>-HSA-FA). TiS<sub>2</sub>, as a new member of the TMD family, has been reported to have a high NIR absorbance which makes it an attractive candidate for PTT.<sup>34–36</sup> Given its potential as a dual-modality therapy nanoagent, its efficacy as a radio-sensitizer is investigated here for the first time. The advantages of the developed nanoplatform TiS<sub>2</sub>-HSA-FA include: 1) improved stability and biocompatibility of TiS2 due to the PEG and HSA modification; 2) great radio-sensitivity; 3) high photothermal effect under NIR laser irradiation; and 4) remarkable tumor cell targeting effect after sequential conjugation with FA. The in vitro and in vivo results demonstrated that TiS2-HSA-FA are a highly effective nanoagent for synergistic photothermal/radiation therapy, which may ultimately prove to be suitable for clinical use.

# **Methods**

#### **Materials**

Titanium disulfide (TiS<sub>2</sub>, Crystal, 99.995%) and Cell counting kit-8 (CCK-8) were purchased from Sigma-Aldrich (St. Louis,

Mo, USA). FA-PEG<sub>5,000</sub>-NHS and CH<sub>3</sub>-PEG<sub>5,000</sub>-NHS were obtained from Xi 'an Kaixin Biotech. Co. Ltd (China). Human serum albumin (HSA) and Fluorescein isothiocyanate (FITC) were obtained from Aladdin (Shanghai, China). Calcein-AM (CA)-propidium iodide (PI) stain were purchased from Sigma-Aldrich (St. Louis, Mo, USA).

# Preparation and characterizations of $Tis_2$ -HSA-FA

In detail, 20 mg bulk TiS<sub>2</sub> was added into 10 mL distilled water, following 2 hrs ultrasonication (2s on and 3s off) in a sonicator Omni Sonic Ruptor 4000 (Omni International, Kennesaw, GA, USA). After that, 10 mg HSA was added to the mixture and sonicated at the same condition for further 6 hrs. After centrifugation at 7000 rpm for 18 mins, the supernatant was collected and centrifuged at 10,000 rpm for 20 mins, resulting in TiS<sub>2</sub> nanosheets solution. Next, 10 mL TiS<sub>2</sub> nanosheets (1 mg/mL) is mixed with FA-PEG<sub>5.000</sub>-NHS (10 mg) and stirred for 2 hrs to be TiS<sub>2</sub>-HSA-FA. As a contrast, FA-PEG<sub>5.000</sub>-NHS was replaced by CH<sub>3</sub>-PEG<sub>5.000</sub>-NHS to form TiS<sub>2</sub>-HSA. Lastly, the resulted mixture was purified by dialysis in distilled water over 24 hrs to obtain TiS2-HSA and TiS2-HSA-FA. The morphology, size, zeta potential, XRD, and UV-VIS spectra of the resulted products were detected on atomic force microscopy (AFM, multimode, digital instruments, Veeco Company, USA), FEI transmission electron microscope (Eindhoven, The Netherlands), ZetaSizer Nano ZS (Malvern Instruments Ltd., UK), X-ray diffractometer (D8 ADVANCE, Bruker, Germany), UV-VIS spectrophotometry (UV-Vis 1800, Shimadzu, Kyoto, Japan), Fourier transform infrared spectroscopy (FT-IR, Bruker Optics GmbH, Ettlingen, Germany), respectively.

# Cell culture

CT26 cells (mice colon cancer cell line) were obtained from Type Culture Collection of Chinese Academy of Science (Shanghai, China). CT26 cells were cultured in RPMI 1640 medium supplemented with 10% fetal bovine serum, 1% penicillin and streptomycin in an atmosphere of 5% CO<sub>2</sub> at  $37^{\circ}$ C.

# Cellular uptake and in vitro biocompatibility

According to previous literatures, a classic small molecule dye, FITC, was applied to label the nanoparticles by simple physical absorption. After 24 hrs incubating, CT26 cells were cultured with free FITC,  $TiS_2$ -HSA,  $TiS_2$ -HSA-FA + FA, and

TiS<sub>2</sub>-HSA-FA for 4 hrs, respectively. And then, the treated cells were successively washed by phosphate buffer saline (PBS) for three time slightly and fixed by glutaraldehyde, stained with DAPI for 10 mins. A commercial confocal laser scanning microscope was used to observe the fluorescence signals inside cells. Moreover, the treated cells were homogenized, and treated with 1 mL aqua regia solution for 5 hrs. An inductively coupled plasma–atomic emission spectrometry (ICP-AES, Hitachi P4010, Japan) was applied to detect the Ti content in the cells.

The in vitro biocompatibility of TiS<sub>2</sub>-HSA and TiS<sub>2</sub>-HSA-FA on cells was evaluated by a standard CCK-8 assay. In detail, CT26 cells ( $1 \times 10^5$  cells/mL, 0.5 mL) were cultured in 96-well plate for 24 hrs and then, the cells were treated with different concentration of TiS<sub>2</sub>-HSA and TiS<sub>2</sub>-HSA-FA. After 24 hrs incubation, the cell viability was detected by CCK-8 assay.

#### In vitro synergistic PTT/RT

CT26 cells were treated with different concentration of  $TiS_2$ -HSA and  $TiS_2$ -HSA-FA (0, 10, 30, 50, 100, 150 µg/mL) and were cultured in 37°C incubator for 5 hrs. After washing the nanoparticles outside the cells, they were irradiated with NIR irradiation (808 nm laser at a power density of 0.8 W/cm<sup>2</sup> for 5 mins) or RT (5Gy), or their combination. And then, the treated cells were further cultured for 24 hrs. During the 5 mins NIR irradiation, a handheld thermal camera (Ti27, Fluke, USA) was used to record the temperature change of the cells. The cell death rate was calculated using a typical CCK-8 assay.

As above, the cells were treated with TiS<sub>2</sub>-HSA and TiS<sub>2</sub>-HSA-FA, following by irradiation with NIR irradiation and X-ray at the same condition. According to the previous literatures, the cells were further stained with calcein-AM/PI and  $\gamma$ -H2AX, respectively, to evaluate the cell death. The fluorescence signal of stained cells was observed by a confocal laser scanning microscope (LSM 510 NLO META, Zeiss, Germany).

#### Animal model

We have revised the ethics statement: All animal experiments were strictly complied with the guideline of Animal Protection and Care Committee of Sichuan University. All animal experimental procedures involved in this work were approved by the Ethics Committee of Sichuan University. For CT26 tumor xenograft models,  $10^6$  CT26 cells in 150 µL PBS were subcutaneously injected into the right back of mice. After 7–10 days of inoculation, the tumor size was detected by a caliper.

#### In vivo synergistic PTT/RT

To investigate the synergistic PTT/RT, tumor-bearing mice were randomly divided into 5 groups (n=5): group 1: control + NIR + RT; group 2: TiS<sub>2</sub>-HSA-FA + RT; group 3: TiS<sub>2</sub>-HSA-FA + NIR; group 4: TiS<sub>2</sub>-HAS + RT+NIR; and group 5: TiS<sub>2</sub>-HSA-FA + RT+NIR (with 6 mg/kg of TiS<sub>2</sub>). NIR irradiation used 808 nm wavelength laser with 0.8 W/cm<sup>2</sup>. RT applied 5 Gy X-ray for 5 mins. The temperature change of the tumor region when irradiated by NIR was recorded using an infrared thermal camera. Every three days treatment, the tumor size was recorded and the tumor volume was calculated according to the equation:  $V = \text{length} \times \text{width}^2/2$ . The relative tumor volume was calculated as  $V/V_0$  (V: current volume,  $V_0$ : initial tumor volume). After the whole treatment, the major organs of these mice were collected for hematoxylin and eosin (H&E) staining. In addition, the blood was collected and the index including white blood cell (WBC), red blood cells (RBC), hemoglobin (HGB), mean corpuscular hemoglobin (MCH), hematocrit (HCT), mean corpuscular hemoglobin concentration (MCHC), mean corpuscular volume (MCV), and platelet (PLT) were detected.

#### Statistical analysis

All data were presented as mean with standard deviation (SD). Statistical analysis was analyzed with OriginPro 2016 via Students's *t*-test. The differences were considered significant for \*P<0.05 and highly significant for \*P<0.01.

# **Results and discussion**

# Preparation and characterization of $TiS_2$ -HSA-Fa

TiS<sub>2</sub> nanosheets were first prepared by HSA-assisted ultrasonication, and their sheet structure was confirmed by AFM image (Figure S1). They were then modified by PEGylated FA to produce TiS<sub>2</sub>-HSA-FA. TEM imaging shows that TiS<sub>2</sub>-HSA-FA has a sheet-like structure with a lattice plane spacing of 0.24 nm (Figure 1A). As shown in Figure 1B, the sharp and narrow XRD peaks in TiS2-HSA-FA indicate good crystallinity of the prepared TiS2-HSA-FA, consistent with observations from HRTEM (Figure 1A, inset). In addition, both bulk TiS<sub>2</sub> and TiS<sub>2</sub>-HSA-FA showed the same phase structure, demonstrating that the exfoliation process has no significant influence on the crystalline structure of the material.<sup>37</sup> According to DLS analysis, the zeta potential and average diameter of TiS2-HSA-FA nanoparticles were approximately -31.2 mV and 135.3 nm, respectively (Figure 1C and D). After 15 days of storage in physiological solution, the size of the

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Figure I Preparation and characterization.

Notes: (A) TEM image of TiS<sub>2</sub>-HSA-FA. Inset was the high-resolution TEM image. (B) XRD pattern of bulk TiS<sub>2</sub> and TiS<sub>2</sub>-HSA-FA. (C) The zeta potential distribution of TiS<sub>2</sub>-HSA-FA. (D) The size distribution of TiS<sub>2</sub>-HSA-FA. (E) The size change of TiS<sub>2</sub>-HSA-FA in physiological solution over 15 days. (F) The absorbance spectra of TiS<sub>2</sub>-HSA-FA. (Abbreviations: TiS<sub>2</sub>, titanium disulfide; HSA, human serum albumin; FA, folic acid; TEM, transmission electron microscopy; XRD, X-ray diffraction.

TiS<sub>2</sub>-HSA-FA nanoparticles displayed no notable changes (Figure 1E). This stability is likely due to the absorption of HSA onto the surface of the particles, and subsequent modification with PEG. The UV-Vis spectrum of TiS<sub>2</sub>-HSA-FA in Figure 1F shows high absorbance across all wavelengths from UV to NIR. The extinction coefficient of TiS<sub>2</sub>-HSA-FA at 808 nm was found to be 30.1 L/g cm. In addition, as shown in Figure S2, the more intense ~1650 cm<sup>-1</sup> peak in TiS<sub>2</sub>-HSA-FA and FA.

# Photothermal effect of TiS<sub>2</sub>-HSA-FA

To test the photothermal properties of TiS<sub>2</sub>-HSA-FA, different concentrations (0, 50, 100, and 150 mg/mL) of the nanoparticles were irradiated by NIR laser (808 nm, 0.8 W/cm) for 5 mins. The results showed that laser irradiation produced significant concentration-dependent temperature increases in TiS<sub>2</sub>-HSA-FA (Figure 2A). The highest temperature that could be reached was 65.3°C. According to previous literatures,<sup>38–40</sup> the photothermal conversion efficiency of TiS<sub>2</sub>-HSA-FA was calculated to be ~58.9%. The photothermal stability of TiS<sub>2</sub>-HSA-FA were clearly very stable throughout five cycles of NIR

irradiation. In addition, the Hounsfield unit values of  $TiS_2$ -HSA-FA, detected by computed tomography, were positively correlated with concentration (Figure 2C), demonstrating that  $TiS_2$ -HSA-FA is a very effective radio-sensitizer.

# Cellular uptake and in vitro biocompatibility

After labeling by FITC, the behavior of  $TiS_2$ -HSA and  $TiS_2$ -HSA-FA in cells was tracked by fluorescence microscopy. The fluorescence images showed that cells treated with  $TiS_2$ -HSA-FA showed much more fluorescence signal in cytoplasm than those treated with  $TiS_2$ -HSA-FA + FA,  $TiS_2$ -HSA, and free FITC (Figure 3A). ICP-AES quantitative analysis confirmed these results (Figure 3B). This indicates that FA conjugation significantly accelerated endocytosis of  $TiS_2$ -HSA-FA. In addition, the in vitro biocompatibility of the  $TiS_2$ -HSA-FA was evaluated by standard CCK-8 assay. As shown in Figure 3C, no significant cytotoxicity of  $TiS_2$ -HSA-FA was found even at high concentrations up to 0.8 mg/mL, indicating good in vitro biocompatibility for both  $TiS_2$ -HSA and  $TiS_2$ -HSA-FA.



Figure 2 The photothermal and radio-sensitization property.

**Notes:** (**A**) Temperature changes of TiS<sub>2</sub>-HSA-FA solution with various concentrations under 808 nm laser irradiation ( $0.8 \text{ W/cm}^2$ ). (**B**) Temperature variations of TiS<sub>2</sub>-HSA-FA under 5 cycles of 808 nm laser irradiation ( $0.8 \text{ W/cm}^2$ ). (**C**) The correlation between HU values and different concentrations of TiS<sub>2</sub>-HSA-FA. The inset is CT images. **Abbreviations:** TiS<sub>2</sub>, titanium disulfide; HSA, human serum albumin; FA, folic acid; CT, computed tomography.



Figure 3 Cell uptake and biocompatibility.

Notes: (A) Fluorescence images of CT26 cells incubated with free FITC and FITC labeled  $TiS_2$ -HSA,  $TiS_2$ -HSA-FA + FA blocking, and  $TiS_2$ -HSA-FA. (B) Quantitative analysis of CT26 cells towards free FITC and FITC labeled  $TiS_2$ -HSA,  $TiS_2$ -HSA-FA + FA blocking, and  $TiS_2$ -HSA-FA (B) Quantitative analysis of CT26 cells towards free FITC and FITC labeled  $TiS_2$ -HSA,  $TiS_2$ -HSA-FA + FA blocking, and  $TiS_2$ -HSA-FA (C) Cell viability of CT26 cells after 24 hrs treatment with different concentrations of  $TiS_2$ -HSA and  $TiS_2$ -HSA-FA.

Abbreviations: TiS<sub>2</sub>, titanium disulfide; HSA, human serum albumin; FA, folic acid; ICP-AES, inductively coupled plasma-atomic emission spectrometry; FITC, fluorescein isothiocyanate; DAPI, 4',6-diamidino-2-phenylindole.

### In vitro synergistic PTT/RT

As shown in Figure 4A, CT26 cells treated with TiS<sub>2</sub>-HSA-FA showed 28.5°C of temperature increase after 5 mins of NIR laser irradiation (808 nm, 0.8 W/cm<sup>2</sup>), which was higher than that of either TiS<sub>2</sub>-HSA-treated or control-treated cells. Since the data from Figure 2C suggested that TiS<sub>2</sub> has potential as a radio-sensitizer, the in vitro RT efficacy of TiS<sub>2</sub>-HSA-FA was tested:

as seen in Figure 4B, cell viability decreased with increasing Xray dose. TiS<sub>2</sub>-HSA-FA + RT exhibited greater inhibition of cell viability than either TiS<sub>2</sub>-HSA-treated or control-treated cells. This is likely because TiS<sub>2</sub>-HSA-FA is more effectively endocytosed, and thus can absorb the energy of X-ray radiation more effectively inside tumor cells and channel it into the formation of secondary Auger electrons to damage DNA.<sup>41–43</sup>



Figure 4 In vitro photothermal radiotherapy.

Notes: (A) Temperature change curve of control, TiS2-HSA and TiS2-HSA-FA under 5 mins NIR irradiation (808 nm, 0.8 W/cm<sup>2</sup>). (B) Cell viability of CT26 cells treated by TiS2-HSA and TiS2-HSA-FA and were irradiated by different dose of X-ray. (C) Cell viability of CT26 cells treated by TiS2-HSA and TiS2-HSA-FA and irradiated by NIR laser or X-ray. (D) Live-dead staining images of CT26 cells treated with PBS, PBS + NIR, TiS2-HSA-FA, TiS2-HSA-FA + NIR. (E)  $\gamma$ -H2AX staining images of CT26 cells treated with PBS + RT, PBS + NIR, TiS2-HSA-FA, TiS2-HSA-FA + NIR, TiS2-HSA-FA + RT, and TiS2-HSA-FA + NIR+ RT, respectively.

Abbreviations: TiS2, titanium disulfide; HSA, human serum albumin; FA, folic acid; RT, radiation therapy; NIR, near infrared; PBS, phosphate buffer saline.

The effect of combined PTT/RT treatment was then investigated. Cells were treated with control + NIR + RT,  $TiS_2$ -HSA-FA + RT,  $TiS_2$ -HSA-FA + NIR,  $TiS_2$ -HAS + NIR + RT, or  $TiS_2$ -HSA-FA + NIR + RT. As shown from the standard CCK-8 assay, under NIR and RT treatment, TiS<sub>2</sub>-HSA-FA displayed the highest cell inhibition rate (93.4%) of all the groups (Figure 4C).

Calcein-AM/PI staining and y-H2AX immunofluorescence were further used to evaluate the combined effect of PTT and RT. The RT- and PTT-treated cells were stained by calcein-AM/ PI. As shown in Figure 4D, almost all the cells were killed in the TiS<sub>2</sub>-HSA-FA + NIR + RT group, while few were killed in the PBS, PBS + NIR, and TiS<sub>2</sub>-HSA-FA groups. Figure 4E shows the results of  $\gamma$ -H2AX immunofluorescence. In PBS + RT, PBS +NIR, TiS<sub>2</sub>-HSA-FA, and TiS<sub>2</sub>-HSA-FA + NIR-treated groups, negligible y-H2AX immunofluorescence was seen. By contrast, the  $TiS_2$ -HSA-FA + RT and  $TiS_2$ -HSA-FA + NIR + RT-treated groups exhibited strong  $\gamma$ -H2AX immunofluorescence signals, suggesting that TiS<sub>2</sub>-HSA-FA can enhance the radio-sensitivity of cells and produce more DNA damage.

#### In vivo biodistribution and blood circulation

Titanium content of the major organs post-injection of TiS<sub>2</sub>-HSA and TiS<sub>2</sub>-HSA-FA were evaluated. The majority of the two nanoparticles were distributed in liver and kidney. Much more TiS2-HSA-FA was collected in tumor tissue than  $TiS_2$ -HSA (Figure 5A). The concentration of  $TiS_2$ -HSA-FA in tumor tissue peaked at 24 hrs post-injection (Figure 5B). The accumulation of TiS<sub>2</sub>-HSA-FA in tumor was likely due to the FA modification, which is known to facilitate tumor targeting.<sup>44,45</sup> As shown in Figure 5C, after intravenous injection, blood distribution half-life  $(t_{1/2}\alpha)$  and blood terminal elimination half-life  $(t_{1/2}\beta)$  of the TiS<sub>2</sub>-HSA-FA were 1.21±0.11 hrs and 17.52±0.62 hrs, respectively. It has been reported that PEG and HSA modifications can prolong blood circulation and reduce macrophage clearance of nanoparticles from the reticuloendothelial system.<sup>46,47</sup>

### In vivo synergistic PTT/RT

For in vivo synergistic PTT/RT, NIR (5 mins, 808 nm, 0.8 W/cm<sup>2</sup>) and X-ray (5 mins, 5Gy) irradiation were applied



Figure 5 In vivo biodistribution and blood circulation.

**Notes:** (**A**) Ti concentration in tumor and major organs (heart, liver, spleen, lung, and kidney) of TiS<sub>2</sub>-HSA-FA-treated mice. (**B**) Ti concentration in tumor region of TiS<sub>2</sub>-HSA-FA-treated mice at different time points. (**C**) Ti concentration in blood at different time points after injection of TiS<sub>2</sub>-HSA-FA. **Abbreviations:** TiS<sub>2</sub>, titanium disulfide; HSA, human serum albumin; FA, folic acid.

24 hrs after intravenous injection. The temperature of the tumor region was recorded by a thermal imager. Figure 6A and B showed a roughly 25°C increase in TiS<sub>2</sub>-HSA-FA + NIR-treated mice, compared to those treated with control or TiS<sub>2</sub>-HAS + NIR. The weight of the mice increased normally over the duration of the 21-day treatment (Figure 7A). The best tumor growth inhibition effect was observed with combined PTT/RT in group 5 (TiS<sub>2</sub>-HSA-FA + NIR+RT). The results demonstrated that PTT/RT delivered by TiS<sub>2</sub>-HSA-FA have an obviously synergistic therapeutic outcome compared to PTT or RT alone (Figure 7B).

After the treatment, the heart, liver, spleen, lung, kidney, and whole blood were collected for HE section staining and complete blood panel assays to evaluate the biocompatibility of the nanoparticles. As seen in Figure 8A and B, no obvious differences were observed between the TiS<sub>2</sub>-HSA-FA group and the control group. This indicates that TiS<sub>2</sub>-HSA-FA has good in vivo biocompatibility.

#### Conclusion

In summary, we have prepared a biocompatible PTT/RT nanoplatform  $TiS_2$ -HSA-FA by using simple ultrasonication to create albumin exfoliated  $TiS_2$  nanosheets that were then modified with PEG and FA. The  $TiS_2$ -HSA-FA nanoparticles showed strong NIR light absorbance, good stability, and remarkable efficacy as a radio-sensitizer. In vitro and in vivo characterization showed  $TiS_2$ -HSA-FA to have a high specificity for targeting tumors, likely due to its modification with FA. The nanoparticles also produced a remarkable, synergistic, cytotoxic effect under PTT/RT irradiation, and showed great biocompatibility in vitro and in vivo. This multifunctional nanoplatform shows great promise for future use as a new tumor therapeutic agent.

#### Disclosure

The authors report no conflicts of interest in this work.



Figure 6 In vivo photothermal performance.

**Notes:** (A) In vivo thermal images of mice after intravenous injection of saline,  $TiS_2$ -HSA and  $TiS_2$ -HSA-FA under 5 mins NIR irradiation (808 nm, 0.8 W/cm<sup>2</sup>). (B) The corresponding temperature change curves of tumor regions in mice.

Abbreviations: TiS<sub>2</sub>, titanium disulfide; HSA, human serum albumin; FA, folic acid; RT, radiation therapy; NIR, near infrared.



Figure 7 In vivo synergistic photothermal radiotherapy.

**Notes:** The change of (**A**) body weight and (**B**) relative tumor volume of CT26-bearing mice in different groups, including control (saline) + NIR+RT, TiS<sub>2</sub>-HSA-FA + RT, TiS<sub>2</sub>-HSA-FA + NIR, TiS<sub>2</sub>-HSA-FA + NIR + RT, and TiS<sub>2</sub>-HSA-FA + NIR + RT.  $\stackrel{**P<0.01}{=}$ , compared to other groups. **Abbreviations:** TiS<sub>2</sub>, titanium disulfide; HSA, human serum albumin; FA, folic acid; RT, radiation therapy; NIR, near infrared.



Figure 8 In vivo biocompatibility.

Notes: (A) HE-stained images of heart, liver, spleen, lung, and kidney collected from mice after 21 days treatment (scale bar =100 µm). (B) Blood biochemistry of mice after 21 days treatment.

Abbreviations: TiS<sub>2</sub>, titanium disulfide; HSA, human serum albumin; FA, folic acid; HE, hematoxylin and eosin; WBC, white blood cell; RBC, red blood cells; HGB, hemoglobin; MCH, mean corpuscular hemoglobin; HCT, hematocrit; MCHC, mean corpuscular hemoglobin concentration; MCV, mean corpuscular volume; PLT, platelet.

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# Supplementary materials



**Figure S1** (A) The AFM image and (B) height analysis of  $TiS_2$  nanosheets. **Abbreviations:** AFM, atomic force microscopy;  $TiS_2$ , titanium disulfide.



**Figure S2** The FT-IR spectrum of TiS<sub>2</sub>-HSA and TiS<sub>2</sub>-HSA-FA. **Abbreviations:** TiS<sub>2</sub>, titanium disulfide; HSA, human serum albumin; FA, folic acid.

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